Provided for non-commercial research and education use. Not for reproduction, distribution or commercial use.



This article appeared in a journal published by Elsevier. The attached copy is furnished to the author for internal non-commercial research and education use, including for instruction at the authors institution and sharing with colleagues.

Other uses, including reproduction and distribution, or selling or licensing copies, or posting to personal, institutional or third party websites are prohibited.

In most cases authors are permitted to post their version of the article (e.g. in Word or Tex form) to their personal website or institutional repository. Authors requiring further information regarding Elsevier's archiving and manuscript policies are encouraged to visit:

http://www.elsevier.com/copyright

Sensors and Actuators B 149 (2010) 221-225

Contents lists available at ScienceDirect



Sensors and Actuators B: Chemical

journal homepage: www.elsevier.com/locate/snb

A reusable DNA biosensor for the detection of genetically modified organism using magnetic bead-based electrochemiluminescence

Debin Zhu, Jinfeng Liu, Yabing Tang, Da Xing*

MOE Key Laboratory of Laser Life Science & Institute of Laser Life Science, College of Biophotonics, South China Normal University, Guangzhou 510631, China

ARTICLE INFO

Article history: Received 8 April 2010 Received in revised form 6 May 2010 Accepted 14 May 2010 Available online 27 May 2010

Keywords: Magnetic bead Electrochemiluminescence DNA biosensor Genetically modified organism

ABSTRACT

A reusable magnetic bead-based electrochemiluminescence (ECL) DNA biosensor for the detection of genetically modified organism (GMO) is proposed. The sensor method consists of immobilization of biotin-probe using streptavidin-coated magnetic beads, hybridization of target DNA with biotin-probe and ruthenium(II) tris-bipyridal (TBR)-probe, detection of target DNA by direct measuring the ECL emission of TBR. The sensor was applied to detect GMO in engineered tobacco samples. Results indicate that the sensitivity of this sensor method was 5 nmol/L of CaMV355 DNA. A stable calibration curve with a wide dynamic range was established. The calibration curve was linear from 5 nmol/L to 5 μ mol/L, thus, made quantitative analysis possible. GM tobacco samples and non-GM tobacco samples were clearly discriminated by the sensor method. Results of the study suggest that the reusable DNA biosensor is a feasible tool for daily GMO detection due to its rapidness, simplicity, safety, sensitivity, reliability and low cost.

© 2010 Elsevier B.V. All rights reserved.

1

SENSORS

ACTUATORS

1. Introduction

Recently, the safety concern of genetically modified organism (GMO) has attracted much attention [1,2]. Many countries require mandatory labeling of GM foods and have adopted a threshold for affirmative GMO labeling (e.g., 0.5% in the European Union) [3]. Hence, demand for testing GM foods has increased dramatically. Polymerase chain reaction (PCR) combined with gel electrophoresis analysis is the most widely used tool for GMO identification [4,5]. However, gel electrophoresis and ethidium bromide (EB) staining are laborious, time-consuming and poisonous. The need for simplicity and speed in these assays has stimulated the development of DNA biosensors for GMO screening, such as quartz crystal microbalance (QCM)-based DNA biosensor [6-8], surface plasmon resonance (SPR) biosensor [9-12], electrochemical genosensor [7,13-15], and nanoparticle-based DNA biosensor [16]. The analytical performances of these biosensors for the detection of GMO are listed in Table 1.

Electrochemiluminescence (ECL), where light-emitting species are produced by reactions between electrogenerated intermediates, has become an important and powerful analytical tool [17–26]. An ECL reaction between ruthenium(II) tris-bipyridal (TBR) and tripropylamine (TPA) has been demonstrated to be a highly sensitive approach to quantify target DNA in our previous study [20]. In the present work, we report a reusable magnetic bead-based ECL DNA biosensor for GMO detection. The cauliflower mosaic virus CaMV35S (CaMV35S) promoter and the nopaline synthase (NOS) terminator commonly used in transgenic products [27] were targeted. As an example, engineered tobacco samples were tested by the sensor.

2. Materials and methods

2.1. Materials

Tobacco samples were gifts from South China Agricultural University, Guangzhou, China. UNIQ-10 column PCR product purification kit was purchased from Shanghai Sangon Biological Engineering Technology & Service Corporation Ltd. (SSBE). Streptavidin-coated magnetic beads (2.8 µm diameter) were products of Dynal Biotech (Lake Success, NY, USA). TPA was purchased from Sigma (Louis, MO, USA). The primers and probes used for GMO detection were synthesized by SSBE. The probes were labeled with biotin by SSBE and labeled with TBR by our laboratory according to Terpetschnig's paper [28]. The sequences of the primers and probes were shown in Table 2.

2.2. Apparatus

The reusable magnetic bead-based ECL DNA biosensor was designed by our laboratory. The heart of it is an electrochemical detection cell, containing a platinum working electrode (disk), a platinum counter electrode (cirque) and an Ag/AgCl reference electrode (thread). A removable magnet is placed under the

^{*} Corresponding author. Tel.: +86 20 85210089; fax: +86 20 85216052. *E-mail address*: xingda@scnu.edu.cn (D. Xing).

^{0925-4005/\$ –} see front matter $\mbox{\sc 0}$ 2010 Elsevier B.V. All rights reserved. doi:10.1016/j.snb.2010.05.047

Author's personal copy

D. Zhu et al. / Sensors and Actuators B 149 (2010) 221-225

Table 1

Comparison of the analytical performances of current biosensors for the detection of GMO.

| Method | Detection limit | Linearity range | Reproducibility | Ref. no. |
|---|--------------------|------------------------------------|-----------------|----------|
| QCM-based DNA biosensor | 0.025 μM | 0–0.1 μM | 10-15% (CV) | [6] |
| SPR biosensor | 1 nM | 1–100 nM for NOS; 1–125 nM for 35S | <3% (CV) | [9] |
| Enzyme-based electrochemical genosensor | 1.2 pM | 12 pM to 12 nM | 10% (SD) | [14] |
| Nanoparticle-based DNA biosensor | 0.8 fmol (0.16 nM) | 0–25 fmol | 2.6–12.2% (SD) | [16] |

working electrode for immobilization and release of the biotinprobe captured by streptavidin-coated magnetic beads. The ECL emission is received by a single photon counting module (MP-962, PerkinElmer, Germany) and the ECL value is output by a personal computer.

2.3. Sample preparation

The genomic DNAs of the tobacco samples were extracted by the cetyltrimethyl ammonium bromide (CTAB) method. Briefly, the sample was minced with sterile surgical blades and dried to flour, then moistened with threefold amount of water and extracted by CTAB, precipitated, treated with chloroform, and precipitated with isopropanol to obtain the purified genomic DNA. The concentration of the genomic DNA was determined by measuring the absorbance at 260 nm (A_{260}) using a UV Spectrophotometer (BioPhotometer, Eppendorf, Germany). The purity of the DNA was determined by calculating the ratio of absorbance at 260 nm to that of 280 nm (A_{260}/A_{280}).

The genomic DNA with an A_{260}/A_{280} ratio of 1.8–2.0 was used as template to amplify the GMO target DNA (CaMV35S promoter and NOS terminator) following the PCR procedure of Pietsch [29]. The thermocycler (PTC-100 MJ Research Inc., USA) was programmed with an initial step of denaturation at 94 °C for 3 min. Cycling conditions were: denaturation at 94 °C for 20 s, annealing at 54 °C for 40 s and elongation at 72 °C for 1 min. In total 40 cycles of above program were performed. The last round of elongation at 72 °C was for 3 min. Negative controls (PCR without DNA template) were processed in parallel with each batch of samples to monitor the possible contamination. The concentration of PCR products was determined spectrophotometrically at 260 nm. Screening of the PCR products was performed by gel electrophoresis and visualized through a UV transilluminator. The PCR products were then diluted 10 times and used as GMO target DNAs for tobacco samples detection.

2.4. Immobilization of biotin-probe

Twenty microliters of biotin-probe and $10 \,\mu$ L of streptavidincoated magnetic beads were incubated at 37 °C for 20 min, to form the biotin-streptavidin linkage. Then, the mixture was added to the electrochemical detection cell and the biotin-probe captured by streptavidin-coated magnetic beads was immobilized on the working electrode by activating the magnetic field of the removable magnet.

Table 2

Primers and probes used for GMO detection.

2.5. Hybridization with GMO target DNA and TBR-probe

Twenty microliters of denatured GMO target DNA and 20 μ L of TBR-probe were added to the electrochemical detection cell in turn, and the mixture was hybridized at 50 °C for 10 min, to form a biotin-probe, GMO target DNA and TBR-probe sandwich complex.

2.6. ECL detection

Tris–EDTA (TE) (pH 7.4) buffer containing TPA was added to the electrochemical detection cell, and a voltage of 1.25 V was applied across the electrode to start the reaction between TBR and TPA, which can emit photons for ECL detection. After ECL detection, the sandwich complex with the magnetic beads was washed away by deactivating the magnetic field. To start the next detection cycle, a new biotin-probe bound to streptavidin-coated magnetic beads was immobilized on the working electrode by reactivating the magnetic field.

2.7. Calibration of the sensor method for CaMV35S target DNA

To prepare the calibration standards, PCR product of CaMV35S promoter was purified using UNIQ-10 column PCR product purification kit, and quantified by absorbance measurement at 260 nm. The purified PCR product was then serially diluted into a series of samples containing different concentrations of CaMV35S target DNA, ranging from 5 nmol/L to 5 μ mol/L. Three separate samples for each CaMV35S concentration were prepared and evaluated by the sensor method. Each sample was measured 30 times with 1-s data integration. The averages and the standard deviations were calculated using Microsoft Excel spread sheet function. The calibration curve was plotted as the ECL value (counts per second, cps) against the CaMV35S concentration.

A threshold value is calculated based on the average (V_{negative}) and standard deviation ($V_{\text{stdev(neg)}}$) of the ECL value from the negative controls (PCR without DNA template), shown as formula (1), to define if a sample was positive of GMO (containing GM component).

$$V_{\text{threshold}} = V_{\text{negative}} + 3V_{\text{stdev(neg)}} \tag{1}$$

3. Results and discussion

3.1. Principle

Fig. 1 shows the basic principle of the reusable magnetic bead-based ECL DNA biosensor for the detection of GMO.

| Name | Sequence (5′–3′) | Product size (bp) | GC content (%) |
|--------------------------|-----------------------------------|---------------------------------------|----------------|
| CaMV35S sense primer | gctcctacaaatgccatca | 195 (sense primer + antisense primer) | 9/19 (47.7%) |
| CaMV35S antisense primer | gatagtgggattgtgcgtca | | 10/20 (50%) |
| NOS sense primer | gaatcctgttgccggtcttg | 180 (sense primer + antisense primer) | 11/20 (55%) |
| NOS antisense primer | ttatcctagtttgcgcgcta | | 9/20 (45%) |
| CaMV35S biotin-probe | cggcagaggcatcttcaacgatggcc-biotin | | 16/26 (61.5%) |
| CaMV35S TBR-probe | TBR-tttccacgatgctcctcgtgggtggg | | 16/26 (61.5%) |
| NOS biotin-probe | ccatctaaataacgtcatgcat-biotin | | 8/22 (36.4%) |
| NOS TBR-probe | TBR-cgcgtattaaatgtataattgcg | | 8/23 (48.2%) |

222

D. Zhu et al. / Sensors and Actuators B 149 (2010) 221-225



Fig. 1. The basic principle of the reusable magnetic bead-based ECL DNA biosensor for the detection of GMO. TBR-probe (*****); biotin-probe (******); streptavidin-coated magnetic beads (•); photon (*).

Briefly, a biotin-probe prebound to the magnetic beads through biotin-streptavidin linkage was immobilized on the working electrode of the electrochemical detection cell by activating the magnetic field of the removable magnet. Then, the GMO target DNA was hybridized with the immobilized biotin-probe and the TBRprobe, forming a sandwich complex, in which TBR reacted with TPA



Fig. 2. System stability of the sensor. Each analysis represents a single run with 30 s acquisition time of each CaMV35S concentration on each day. Error bars indicate standard deviations from 30 s acquisition time.



Fig. 3. Calibration curve for the detection of CaMV35S. The calibration curve was obtained by measuring a series of purified CaMV35S amplicon concentration from 5 nmol/L to $5 \mu \text{mol/L}$.

to emit light for ECL detection. After ECL detection, the sandwich complex with the magnetic beads was washed away by deactivating the magnetic field. To start another detection cycle, a new biotin-probe prebound to streptavidin-coated magnetic beads was immobilized on the working electrode by reactivating the magnetic field.

3.2. Baseline

The negative controls (PCR without DNA template) of CaMV35S and NOS were analyzed by the sensor method. The average ECL value was 17.6 cps for CaMV35S and 18.2 cps for NOS, with a standard deviation of 1.5 cps for CaMV35S and 1.7 cps for NOS. Based on formula (1), we estimated the threshold value is 22.1 cps for CaMV35S and 23.3 for NOS.

3.3. System stability

To estimate the system stability of the sensor, three separate samples for each CaMV35S concentration (ranging from 5 nmol/L to 5 μ mol/L) were prepared and each sample was measured 30 s with one-second data integration. The detection results are shown in Fig. 2. Each bar represents an average value based on 30 s measurements from the same sample, with the error bar (standard deviation) reflecting the measurement variation of the system.



Fig. 4. Detection of the GMO target DNA (CaMV35S and NOS fragments) by the sensor method. The broken lines represent the threshold value for CaMV35S.

Author's personal copy

D. Zhu et al. / Sensors and Actuators B 149 (2010) 221-225



Fig. 5. Detection of the GMO target DNA (CaMV35S and NOS fragments) by 2% agarose gel electrophoresis and EB staining. M, 100-bp DNA markers; NC, negative control; 1, Huayeqing (non-GM tobacco); 2, K306-2 (GM tobacco); 3, K306-13 (GM tobacco); 4, G28-1 (GM tobacco).

The variations in ECL values, among the three separately prepared samples at each CaMV35S concentration level, reflect the variations introduced by an operator during each assay. It can be concluded, based on the data, that the system stability is rather consistent.

3.4. Calibration

A calibration curve for CaMV35S promoter was obtained by measuring a series of denatured purified CaMV35S PCR product samples containing different concentrations of CaMV35S target DNA, as shown in Fig. 3. The data show a linear relationship between the ECL value and the target DNA concentration range from 5 nmol/L to 5 μ mol/L (R^2 = 0.9971). The calibration curve can be used for quantitative analysis of GM component.

On the basis of the calibration curve, a conservative estimate gives rise to a sensitivity of 5 nmol/L, below which the ECL value approaches the detection threshold value of 22.1 cps. Though the sensitivity of our biosensor is lower than the SPR biosensor [9–12], electrochemical genosensor [7,13–15] and nanoparticle-based DNA biosensor (as shown in Table 1), it is sufficient for GMO detection since the concentration of GMO PCR product is usually nmol/L levels.

3.5. Detection of tobacco samples by the sensor

Different tobacco samples were detected by the sensor method. Results are shown in Fig. 4. The average ECL value of non-GM tobacco (Huayeqing) was 7.4 ± 0.6 cps (average \pm standard deviation) for CaMV35S and 15.1 ± 1.2 cps for NOS, both of them were under the threshold values. The average ECL values of three kinds of GM tobacco samples were 267.1 ± 13.7 cps (CaMV35S) and 237.1 ± 12.3 cps (NOS) for K306-2 tobacco, 398.5 ± 21.3 (CaMV35S) and 380.6 ± 20.5 (NOS) for K306-13 tobacco, and 229.4 ± 12.1 (CaMV35S) and 428.3 ± 21.6 (NOS) for G28-1 tobacco. All of these values were over the threshold values. Most importantly, the signal-to-noise ratio of the detection was higher than 15 times. Therefore, GMO components can be clearly detected by the sensor.

3.6. Accuracy of the sensor method

To verify the accuracy of the sensor method, GMO target DNA (PCR amplified CaMV35S (195-bp) and NOS (180-bp) fragments from tobacco samples) were analyzed by 2% agarose gel electrophoresis and EB staining for comparison. The results are shown in Fig. 5. Both bands of 195 and 180-bp appeared in the lanes of GM tobacco clearly, while no bands were found in non-GM tobacco or negative control. This result is consistent with the result detected

by the sensor, demonstrating a remarkable accuracy of the sensor method.

When developing the sensor method, two probes specific for CaMV35S promoter or NOS terminator were carefully designed. The two different hybridizations in the detection process should significantly limit the false positives. Hence, the detection result by the sensor is specific and reliable, as demonstrated by gel electrophoresis analysis (Fig. 5). Further more, without using the time-consuming gel electrophoresis and EB staining that were commonly used in traditional PCR-based DNA detection, the detection process by the sensor is rapid, simple and safe.

Zhang et al. reported an ECL-based DNA biosensor fabricated by self-assembling the ECL probe of thiolated DNA tagged with ruthenium complex on the surface of a gold electrode [26]. Though their sensor method provides a highly selective tool for target DNA detection, the immobilization of the thiolated DNA probe and the regeneration of the electrode surface were complicated and time-consuming. Recently, the surface-functionalized magnetic beads have been widely used in immune and nucleic acid assays due to its ability to fast separate and preconcentrate low-abundant target analytes (DNA, bacteria, protein) [30,31]. In our study, we introduce the streptavidin-coated magnetic beads for circular immobilization and release of the biotin-probe, thus makes the sensor reusable. Consequently, the detection cost is greatly reduced. Compared with the thiol-derivative process, the magnetic bead-based immobilization and regeneration process is simple and rapid, only need to activate or deactivate the magnetic field.

4. Conclusions

In conclusion, a reusable magnetic bead-based ECL DNA biosensor for GMO detection is developed. The sensor makes the detection of GMO rapid, simple, inexpensive, safe, sensitive and reliable. It can potentially become a convenient tool for daily GMO detection, as well as of other specific nucleic acids.

Acknowledgments

This research is supported by the National Natural Science Foundation of China (30600128), the Natural Science Foundation of Guangdong Province (7005825), the Program for Changjiang Scholars and Innovative Research Team in University (IRT0829), the Key Program of NSFC-Guangdong Joint Funds of China (U0931005), the National Basic Research Program of China (2010CB732602), and the National High Technology Research and Development Program of China (863 Program) (2007AA10Z204).

Author's personal copy

D. Zhu et al. / Sensors and Actuators B 149 (2010) 221-225

References

- F.E. Ahmed, Detection of genetically modified organisms in foods, Trends Biotechnol. 20 (2002) 215–223.
- [2] W.E. Huffman, Production, identity preservation and labeling in a market place with genetically modified (GM) and non-GM foods, Plant Physiol. 134 (2004) 3–10.
- [3] Regulation (EC) No. 1829/2003 of the European Parliament and of the Council of 22 September 2003, See Official Journal of the European Union L 268, 18/10/2003.
- [4] S. Vollenhofer, K. Burg, J. Schmidt, H. Kroath, Genetically modified organisms in food-screening and specific detection by polymerase chain reaction, J. Agric. Food Chem. 47 (1999) 5038–5043.
- [5] M. Lipp, A. Bluth, F. Eyquem, L. Kruse, H. Schimmel, G. Van den Eede, E. Anklam, Validation of a method based on polymerase chain reaction for the detection of genetically modified organisms in various processed foodstuffs, Eur. Food Res. Technol. 212 (2001) 497–504.
- [6] I. Mannelli, M. Minunni, S. Tombelli, M. Mascini, Quartz crystal microbalance (QCM) affinity biosensor for genetically modified organisms (GMOs) detection, Biosens. Bioelectron. 18 (2003) 129–140.
- [7] M. Minunni, S. Tombelli, E. Mariotti, M. Mascini, M. Mascini, Biosensors as a new analytical tool for detection of genetically modified organisms (GMOs), Fresenius J. Anal. Chem. 369 (2001) 589–593.
- [8] I. Karamollaoglu, H.A. Öktem, M. Mutlu, QCM-based DNA biosensor for detection of genetically modified organisms (GMOs), Biochem. Eng. J. 44 (2009) 142–150.
- [9] E. Mariotti, M. Minunni, M. Mascini, Surface plasmon resonance biosensor for genetically modified organisms detection, Anal. Chim. Acta 453 (2002) 165–172.
- [10] R. Wang, S. Tombelli, M. Minunni, M.M. Spiriti, M. Mascini, Immobilization of DNA probes for the development of SPR-based sensing, Biosens. Bioelectron. 20 (2004) 967–974.
- [11] G. Feriotto, M. Borgatti, C. Mischiati, N. Bianchi, R. Gambari, Biosensor technology and surface plasmon resonance for real-time detection of genetically modified Roundup Ready soybean gene sequences, J. Agric. Food Chem. 50 (2002) 955–962.
- [12] E. Giakoumaki, M. Minunni, S. Tombelli, I.E. Tothill, M. Mascini, P. Bogani, M. Buiatti, Combination of amplification and postamplification strategies to improve optical DNA sensing, Biosens. Bioelectron. 19 (2003) 337–344.
- [13] B. Meric, K. Kerman, G. Marrazza, I. Palchetti, M. Mascini, M. Ozsoz, Disposable genosensor, a new tool for the detection of NOS-terminator, a genetic element present in GMOs, Food Control 15 (2004) 621–626.
- [14] F. Lucarelli, G. Marrazza, M. Mascini, Enzyme-based impedimetric detection of PCR products using oligonucleotide-modified screen-printed gold electrodes, Biosens. Bioelectron. 20 (2005) 2001–2009.
- [15] G. Carpini, F. Lucarelli, G. Marrazza, M. Mascini, Oligonucleotide-modified screen-printed gold electrodes for enzyme-amplified sensing of nucleic acids, Biosens. Bioelectron. 20 (2004) 167–175.
- [16] D.P. Kalogianni, T. Koraki, T.K. Christopoulos, P.C. Ioannou, Nanoparticle-based DNA biosensor for visual detection of genetically modified organisms, Biosens. Bioelectron. 21 (2006) 1069–1076.
- [17] G. Xu, S. Dong, Electrochemiluminescent determination of perchlorate by solvent extraction in the presence of Ru(bpy)₃²⁺, Electrochem. Commun. 1 (1999) 463–466.
- [18] X. Chen, M.J. Li, C.Q. Yi, Y. Tao, X.R. Wang, Electrochemiluminescence determination of nitro polycyclic-aromatic hydrocarbons using HPLC separation, Chromatographia 58 (2003) 571–577.
- [19] M.M. Richter, Electrochemiluminescence (ECL), Chem. Rev. 104 (2004) 3003–3036.

- [20] D.B. Zhu, D. Xing, X.Y. Shen, J.F. Liu, Q. Chen, High sensitive approach for point mutation detection based on electrochemiluminescence, Biosens. Bioelectron. 20 (2004) 448–453.
- [21] Z. Lin, J. Sun, J. Chen, L. Guo, G. Chen, Enhanced electrochemiluminescent of lucigenin at an electrically heated cylindrical microelectrode, Electrochem. Commun. 9 (2007) 269–274.
- [22] H. Wei, Y. Du, J. Kang, E. Wang, Label free electrochemiluminescence protocol for sensitive DNA detection with a tris(2,2'-bipyridyl)ruthenium(II) modified electrode based on nucleic acid oxidation, Electrochem. Commun. 9 (2007) 1474–1479.
- [23] H. Hiroki, S. Wataru, F. Junji, S. Hiroaki, On-chip handling of solutions and electrochemiluminescence detection of amino acids, Sens. Actuators B 122 (2007) 542–548.
- [24] Y. Tao, Z.J. Lin, X.M. Chen, X.L. Huang, M. Oyama, X. Chen, X.R. Wang, Functionalized multiwall carbon nanotubes combined with bis(2,2'-bipyridine)-5-amino-1,10-phenanthroline ruthenium(II) as an electrochemiluminescence sensor, Sens. Actuators B 129 (2008) 758–763.
- [25] W. Miao, Electrogenerated chemiluminescence and its biorelated applications, Chem. Rev. 108 (2008) 2506–2553.
- [26] J. Zhang, H. Qi, Y. Li, J. Yang, Q. Gao, C. Zhang, Electrogenerated chemiluminescence DNA biosensor based on hairpin DNA probe labeled with ruthenium complex, Anal. Chem. 80 (2008) 2888–2894.
 [27] M. Zhang, X. Gao, Y. Yu, J. Ao, J. Qin, Y. Yao, Q. Li, Detection of roundup ready
- [27] M. Zhang, X. Gao, Y. Yu, J. Ao, J. Qin, Y. Yao, Q. Li, Detection of roundup ready soy in highly processed products by triplex nested PCR, Food Control 18 (2007) 1277–1281.
- [28] E. Terpetschnig, H. Szmacinski, H. Malak, J.R. Lakowicz, Metal–ligand complexes as a new class of long-lived fluorophores for protein hydrodynamics, Biophys. J. 68 (1995) 342–350.
- [29] K. Pietsch, U. Waiblinger, P. Brodman, A. Wurz, Screening verfahren zur identifizierung "gentechnisch veranderter" pflanzlicher Lebensmittel, Deutsche Lebensmittel-Rundschau 93 (1997) 35–38.
- [30] F.G. Pérez, M. Mascini, I.E. Tothill, A.P.F. Turner, Immunomagnetic separation with mediated flow injection analysis amperometric detection of viable *Escherichia coli* O 157, Anal. Chem. 70 (1998) 2380–2386.
- [31] G.H. Yan, D. Xing, S.C. Tan, Q. Chen, Rapid and sensitive immunomagneticelectrochemiluminescent detection of p53 antibodies in human serum, J. Immunol. Methods 288 (2004) 47–54.

Biographies

Debin Zhu is an associate professor at South China Normal University. She received her PhD in Optics from South China Normal University in 2005. Her current research interests are electrochemiluminescence-based biosensors and applications of nanomaterials in biological systems.

Jinfeng Liu received his MS degree in Optics from South China Normal University in 2005. He works for a biotechnology company currently and his interest is in optical imaging.

Yabing Tang received his MS degree in Optics from South China Normal University in 2007. He works for a biotechnology company currently and his interests include specific nucleic acids sequences analysis and detection of pathogenic bacteria in plants with electrochemiluminescence systems.

Da Xing is a professor at South China Normal University. He received his PhD in Engineering from Harbin Institute of Technology in 1990. His current research interest is the applications of laser spectroscopy in molecule biology.